# **A Review of Online Adaptive Radiation Therapy**

Lan Lu, PhD; Zhexuan Zhang, PhD; Peng Qi, PhD\*

# Abstract

Advances in cone-beam CT (CBCT) and MRI, together with rapid and accurate tissue segmentation and treatment planning accelerated by artificial intelligence and machine learning, have made online adaptive radiation therapy (ART) feasible on commercial radiation therapy systems. In this review, we examine the status of CBCT- and MRI-based online ART in light of their recent increase in clinical adoption.

Keywords: adaptive radiation therapy, CBCT, MRI

# Introduction

With technology advancements and contour standardization, errors in imaging, contouring, and treatment setup have been reduced over the last decades. However, errors occur when a singular treatment plan is used over the course of therapy without adjustment for the patient's anatomical changes during that time. Yan proposed the concept of adaptive radiation therapy (ART) to reduce the impact of anatomical changes during therapy and summarized ART as "a closed loop radiation treatment process where the treatment plan can be modified (including re-optimized) using systematic feedback of measurements (e.g., onboard imaging)."1 The goal of ART is to maintain objectives of the initial planning over the course of treatment, during which anatomical change may occur.

Anatomical variations between the initial planning and treatment phases are common in radiation therapy for cancers such as head and neck (HN), lung, prostate, and gastrointestinal cancers. Such variations present in different formats (e.g., tumor shrinkage or progression) and timescale (days to weeks). For example, Kishan et al studied 12 patients with HN and observed a median increase of 16% in the gross target volume between treatment planning and the first treatment (a median of 13 d).<sup>2</sup> Other anatomical changes, such as bladder or rectal filling, peristalsis, and uterus motion, may occur over minutes to hours. Importantly, anatomical variations are often patient-specific and cannot be accurately predicted from population models, warranting the need for ART approaches that can

Affiliations: Department of Radiation Oncology, Taussig Cancer Center, Cleveland Clinic, Cleveland, OH. Corresponding author: \*Peng Qi, PhD, Department of Radiation Oncology, Taussig Cancer Center, Cleveland Clinic 9500 Euclid Ave. CA50, Cleveland, OH 44195. (qip@ccf.org)

**Disclosures:** The authors have no conflicts of interest to disclose. None of the authors received outside funding for the production of this original manuscript and no part of this article has been previously published elsewhere.

Published: January 1, 2025. https://doi.org/10.37549/ARO-D-24-00037

@Anderson Publishing, Ltd. All rights reserved. Reproduction in whole or part without express written permission is strictly prohibited.

respond to an individual patient's evolving anatomy.

A critical component of ART is onboard imaging (OBI). Ideally, the image quality of OBI should be comparable to that of simulation to ensure accurate adaptation. However, compared with simulation CT (SIM-CT), OBI on a regular linear accelerator (linac), cone-beam CT (CBCT) system produces inferior images that can be characterized by lower soft tissue contrast, greater susceptibility to artifacts, and inaccurate electron density-to-Hounsfield Unit (HU) calibration.

CBCT technology has been improving due to hardware and software advancements. For example, the gantry speed of a Halcyon linac (Varian Medical Systems, Palo Alto, CA) can reach up to 4 rotations per minutes (RPM), which is 4 times faster than that of a Varian TrueBeam linac. This fast rotation allows for a CBCT acquisition within a single breath-hold (BH).<sup>3</sup> The rapid image acquisition, along with an advanced iterative CBCT (iCBCT) reconstruction algorithm, improved image quality and consistency of BH-CBCTs.<sup>3</sup> Most recently, Varian introduced the HyperSight CBCT system, making the imaging quality of OBI closer to that of SIM-CT.<sup>4,5</sup> The HyperSight is available for the Varian Ethos system (developed based on the Halcyon system), a platform specifically designed for online ART.

CBCT produces inferior soft tissue contrast compared to MRI. Therefore, a radiation therapy machine equipped with onboard MRI is more desirable for ART, despite the many technical challenges involved in operating the machine in the presence of a strong magnetic field. The first commercial MRI-guided radiation therapy (MRgRT) machine was developed by ViewRay (ViewRay Inc, Oakwood, USA), combining a 0.35 T MRI scanner and 3 Co-60 sources mounted on a ring gantry.<sup>6</sup> In its later design, the Co-60 sources were replaced by a linac for improved treatment effeciency.7 The Elekta Unity MRI-linac (Elekta, Stockholm, Sweden), FDA cleared in 2023, integrates a 1.5 T MRI scanner with a linac.

In this review, we begin with an overview of offline and online ART before focusing on CBCT- and MRI-based online ART. For CBCTbased online ART, we discuss the workflow, advantages, as well as limitations and futures of the Ethos system. For MRI-based online ART or adaptive MRgRT, we also cover its workflow, advantages and limitations, and conclude with our perspectives on the future of online adaptive MRgRT.

# **Offline and Online ART**

Onboard CBCT may capture progressive anatomical changes, such as tumor progression or shrinkage or those caused by weight loss, enabling the use of offline ART when these changes exceed certain thresholds.<sup>1</sup> Offline ART requires replanning between treatment fractions. Because CBCT lacks the image quality (e.g., artifacts, small field of view, inaccurate HU) needed for treatment planning, repeat simulation is required for offline ART. After resimulation, the workflow of offline ART is similar to that of the initial treatment planning: contouring, planning, physician and physicist review, patient-specific quality assurance (PSQA), pretreatment CBCT verification and correction, and treatment delivery.8-10 By combining the delivered fractions with the offline-adapted plans, the overall quality of the radiation therapy can be evaluated. Institutional studies and clinical trials, especially in the treatment of prostate cancer and HN cancer, have shown the benefits of offline ART.<sup>11-14</sup> Additionally, repeated functional imaging can be acquired and used to guide dose adjustments based on tumor responses.<sup>15-18</sup> The frequency of offline ART depends on the timescale and magnitude of anatomical variations.

Online ART involves replanning while patients remain in the treatment position. This approach can be further divided into 2 subcategories: plan-of-the-day (PotD) and daily replanning. The PotD method involves creating a library of plans to accommodate potential daily anatomical variations.<sup>19-23</sup> The physician then selects one plan from the library based on the "daily" anatomy of the pretreatment CBCT. The ART using the PotD strategy is also called hybrid ART because the adaptive plan is created offline but the decision for ART is made online. The method of daily replanning requires potential replanning before treatment.9 The replanning is triggered if target coverage and/or doses to organs-at-risk (OARs) exceed clinically acceptable errors (mostly by physician's decision). By default, daily

replanning strategy is referred to as online ART, which we will focus on in this review.

Despite potentially better patient outcomes, online ART is more time-consuming and resourceintensive than conventional RT or offline ART.<sup>10,23-31</sup> A dedicated team is required to quickly and accurately review and approve daily contours and new plans, and to conduct QAs.

Appropriate patient selection is critical to the success of online ART, which is well suited for cases with noticeable inter-fractional but few intra-fractional anatomical variations. Real-time ART,<sup>32,33</sup> beyond the scope of this review, could be useful for mitigating the impacts of fast intra-fractional tissue variations.

## **CBCT-Based Online ART**

The Varian Ethos system provides a platform to perform online ART in as little as 15 minutes, which is achieved by using rapid, highquality CBCT, as well as artificial intelligence (AI) and machine learning (ML).<sup>34-37</sup>

The Ethos system uses a fast gantry (4 RPM) and a novel iterative (iCBCT) reconstruction method to generate high-quality CBCT.<sup>37,38</sup> It employs AI and ML to expedite tissue segmentation and plan optimization and GPUs to accelerate dose calculations. The Ethos system is an O-ring linac equipped with a 6 MV Flattening Filter Free beam at a maximum dose rate of 800 monitor units per minute (MU/min).<sup>37</sup> A dual-layer multileaf collimator allows for the delivery of both intensity-modulated radiation therapy and volumetric-modulated arc therapy.

#### Workflow

The workflow of online ART on the Ethos system starts with an approved treatment plan called the "reference plan." At each treatment session, a CBCT is acquired that can be reconstructed using iCBCT or a conventional Feldkamp-Davis-Kress (FDK) algorithm. For adaptive, or "intent" planning, a certain set of contours called "influencers" are automatically generated using either an AI-based or deformable image registration (DIR)-based method. The influencer structures are typically structures near or within the target. A structure-guided DIR is applied from the planning CT to the CBCT to create a synthetic CT (sCT) for dose calculation. After the influencer review, target volumes may be propagated onto the pretreatment CBCT and reviewed by the physician. The Ethos system then generates 2 types of plans: a "scheduled plan" by calculating the fluence from the reference plan onto the sCT and an "adaptive plan" using an intelligent optimization engine with the "daily" contours. The physician compares the scheduled and adaptive plans in terms of dose-volume histogram (DVH) metrics and dose distributions, and decides which plan is used for treatment. Subsequently, a qualified medical physicist performs the MU verification using Varian Mobius3D. An optional CBCT can be acquired to verify the final treatment position and evaluate for changes in internal anatomy. Table 1 provides the summary of the workflow of nonadaptive and adaptive planning after the acquisition of SIM-CT.

#### **Advantages**

The Ethos system uses onboard CBCT for ART. Because CBCT is widely used for imageguided radiation therapy, the implementation of Ethos online ART may not require major changes to the existing infrastructure or neecessitate staff training on a completely new technology like MRI-based online ART.

The Ethos iCBCT offers a higher contrast-to-noise ratio than

conventional CBCT, enabling an improved accuracy in soft tissue delineation and dose calculation. The Ethos 2.0 with HyperSight CBCT further enhances its iCBCT performance with faster acquisition time (6 s), a larger field of view (up to 70 cm), and a newly designed kV detector. Users may directly replan on HyperSight iCBCT, eliminating the need for sCT.

Many centers have implemented online ART using the Ethos system for many disease sites<sup>14,26,27,29,35-44</sup> and have shown improved target and/or OAR sparing. For a study in advanced pancreatic cancer, Schiff found that 100% of adapted fractions (40) met the OAR constraints while only 1 out of 40 nonadapted fractions met all OAR constraints.<sup>44</sup> In addition, the Ethos system allows for safe dose escalation in certain cases, which could potentially lead to improved tumor control rates. For online ART, the Ethos system is more cost-effective and offers shorter treatment than MRI-based systems.

# Current Challenges and Future Perspectives

The implementation of online ART using the Ethos system is different from conventional CBCT-guided RT in terms of software, hardware, and workflows. The new approach requires considerable resources (especially in personnel) and thus presents a great challenge for its adoption.<sup>37</sup> Because online ART requires skilled staff to rapidly and accurately assess a patient's daily anatomical changes, make appropriate plan adjustments, and ensure QA during the treatment session, at least one dedicated medical physicist should be present for the majority of the workday to accommodate patient load.<sup>37,43</sup> A physician needs to be present for plan and contour review and approval.

Although AI and automation improve the efficiency of online

ART on Ethos, the treatment can take more than 30 minutes for certain disease sites and for specific patients. The prolonged time on the couch may result in changes to the patient's anatomy, requiring the process to be restarted in the worst scenario.

The Ethos system operates as a black box, and some QA methods for regular linacs are not available . Many built-in QA tools are from Varian (e.g., Mobius3D). Although, retrospectively, the dosimetric and contouring accuracy has been verified,<sup>43,45</sup> there is a need for independent and quick QA solutions for plan checks and secondary dose calculations to guarantee patient safety and treatment accuracy.<sup>46</sup>

Although several studies have demonstrated the dosimetric advantages of online ART in terms of improved target coverage and reduced dose to OARs, more robust prospective clinical trials are needed to establish the impact of online ART on treatment outcomes. Future research also needs to focus on identifying which patient populations and disease sites would benefit most from online ART to optimize resource allocation and ensure cost-effectiveness.<sup>47</sup>

#### **MRI-Based Online Adaptation**

Recent technology advancements have made MRgRT a reality by integrating an MRI scanner with a linac or a Co-60 machine.<sup>48</sup> The first commercial MRgRT system, the ViewRay MRIdian system, was installed at Washington University in St. Louis, and the treatment of patients started in January 2014.6 This machine combined a 0.35 T superconducting MRI scanner with 3 Co-60 heads mounted on a ring gantry, with MRI and RT system sharing the same isocenter. Later models of the MRIdian replaced the Co-60 design with

	NONADAPTIVE	ADAPTIVE
Image registration	Rigid registration between the daily CBCT and the SIM-CT	DIR-based registration between the daily CBCT and the SIM-CT
Contour updates	DIR- or Al-based daily contours	DIR- or AI-based daily contours
Optimization	NO	Plan is reoptimized based on the updated "daily contours"
Plan adaptation	Plan is calculated using the fluence of the original plan on the sCT	Plan is recalculated on the sCT after optimization

a linac for enhanced treatment capabilities. In 2017, the first person was treated using the MRIdian linac system .<sup>7</sup> Another commercial MRgRT system, the Elekta Unity, was developed by Elekta in partnership with Philips (Philips, Amsterdam, the Netherlands).<sup>49</sup> It integrates a 1.5 T MRI scanner with a linac equipped with 6 MV beams. The higher magnetic field strength produces diagnosticquality imaging. With other systems in the development phase,<sup>50,51</sup> MRgRT introduces a new paradigm in treatment planning, real-time monitoring, and online ART.52,53

## Workflow

An efficient workflow is essential for implementing online adaptive MRgRT. After the target and OAR delineation on CT or MR simulation, a reference plan is created to meet the dosimetric criteria. At each treatment session, a daily MRI is acquired prior to the treatment. According to the anatomy changes in the target and OARs between the pretreatment MRI and simulation image, one of the two workflows can be executed. If the anatomy of target and OAR is sustained, the "adapt to position" workflow is applied. The daily MRI is first aligned with the simulation image based on rigid

registration, and an isocenter shift is implemented. The couch is then translated for the ViewRay system or a virtual couch shift is utilized for the Unity system. If necessary, an adaptive plan can be generated by applying segment adaptation or optimization to further enhance plan dosimetry. These adaptive plans are still based on the simulation images. However, if the anatomical changes are significant, the second method, "adapt to shape," is applied.54-56 The daily MRI and simulation images are first aligned using deformable registration. The original ROIs and plan are propagated to the daily MRI, and new contours of the target and OARs are modified or delineated on the daily MRI. The electron density is assigned to each organ on the MRI generated sCT, and an adaptive plan is generated by adjusting or re-optimizing fluence. A summary of the above adaptive workflows is listed in Table 2.

## Advantages

With superior soft tissue contrast and continuous intrafractional imaging, an MRgRT system could be ideal for online ART.<sup>54-58</sup> Studies show that physicians prefer reoptimized plans in over 90% of cases.<sup>59,60</sup> Unlike CBCT, MRI is nonionizing radiation, enhancing patient safety for treatments requiring frequent imaging. Moreover, MRgRT enables physicians to directly monitor tumor motion without relying on surrogates, reducing alignment errors particularly in areas prone to movement (e.g., abdomen and thorax). This capability allows more precise dose delivery to the target while sparing surrounding healthy tissues, resulting in fewer side effects. For example, patients with prostate cancer treated with online adaptive MRgRT experienced lower rates of gastrointestinal and genitourinary toxicity than those treated with conventional approaches.<sup>61-63</sup> Emerging data suggest that online adaptive MRgRT enables safe dose escalation in the treatment of pancreatic, prostate, and lung cancer.64-68

Because onboard MRI provides accurate volumetric imaging for each treatment, it enables precise calculation of the cumulative dose to organs from each fraction. This detailed volumetric dose mapping allows clinicians to monitor dose constraints and make adjustment if limits are exceeded.<sup>69,70</sup> Understanding the exact dose distribution of organs and their specific subregions is essential for assessing potential toxicities. Voxel-by-voxel data of daily dose offer valuable insights into normal tissue tolerance.71,72

Beyond current MRgRT, functional MRI on an MRI-linac enables the potential of biological guidance RT. Studies indicate that conventional RT can leave radioresistant portions of the tumor undertreated due to tumor heterogeneity, contributing to recurrence.<sup>73</sup> Online adaptive functional MRgRT allows clinicians to obtain biological insights on specific subvolumes within the tumor, facilitating patientspecific, heterogeneous dosing strategies that potentially improve therapeutic outcomes.<sup>74-76</sup>

	ADAPT TO POSITION	ADAPT TO SHAPE
Image registration	Align the daily MRI rigidly to the SIM-CT	Align the daily MRI deformably to the SIM-CT
Contour updates	Use original contours with updated ISO	<ul> <li>Use adapted contours</li> <li>Assign electron density based on the daily MRI</li> </ul>
Segment or fluence optimization	<ul> <li>Use the original segments</li> <li>Adapt the segments</li> <li>Optimize segments' weights</li> </ul>	<ul><li>Optimize fluence weights</li><li>Adjust fluence shape</li></ul>
Plan adaptation	Recalculate or reoptimize the original plan on the SIM-CT	Recalculate or reoptimize the plan on the online MRI
Abbreviations: SIM-CT, simulation CT.		

## Table 2. Workflows of "Adapt to Position" and "Adapt to Shape" in Adaptive MRI-Guided Radiation Therapy

#### **Current Challenges**

Implementing an online adaptive MRgRT program demands considerable investment in capital (significantly more than the in the Ethos system) and personnel, which presents a substantial barrier to its adoption.<sup>61,77</sup>

Integrating an MRI scanner with a linac is complex and comes with inherent limitations. Both components require modification from their conventional forms, resulting in compromised performance compared with their stand-alone counterparts.53,78 Commercial MRI-linacs use lower magnetic field strength than diagnostic MRI scanners (1.5 T to 7 T) to mitigate the electron return effect,<sup>79</sup> resulting in inferior image quality. Because the moving linac gantry disrupts magnetic field homogeneity, most MRI-linacs only allow step-and-shoot delivery.49,80 Additionally, beam configuration is restricted to coplanar angles due to system geometry and beam energy is limited to low energies such as Co-60, 6 MV, and 7 MV.

Another critical concern for online adaptive MRgRT is image distortion as accurate volumetric target delineation and precise location mapping are essential for beam positioning. The MRI scanner in an MRIlinac requires larger volumetric coverage and off-isocenter imaging than a diagnostic scanner, which complicates achieving a homogeneous magnetic field.<sup>81-83</sup> Image distortion is less pronounced at 0.35 T,<sup>56</sup> but in high-field systems like the 1.5 T Elekta Unity, it becomes a greater challenge. Techniques such as field correction, B0 mapping, and local shimming can improve image quality, although shimming becomes particularly challenging with moving components like the gantry.7,53

Online adaptive MRgRT is time-consuming not only because MRI is inherently slow but also due to the multistep adaptation process. Studies indicate that online adaptation can extend RT sessions by 30 to 60 minutes, impacting treatment efficiency and thus throughput.<sup>84,85</sup> Like CBCT-based ART, the extended duration may also increase patient discomfort and the risk of undesired intra-fractional motion, potentially compromising the accuracy of replanning. Given its low cost-effectiveness, appropriate patient selection is crucial. Patients who are most likely to benefit should be prioritized for MRgRT, such as those with tumors that are difficult to visualize or

delineate using CBCT or are located near critical structures.

#### **Future Perspectives**

One promising direction for adaptive MRgRT involves the use of quantitative MRI-derived biomarkers, which can provide valuable insights into treatment response and enable more personalized radiation therapy for potentially improving outcomes. Dynamic contrast-enhanced MRI, which measures tissue perfusion and permeability, allows clinicians to detect microvascular changes that could indicate early responses or resistance to treatment.86,87 This technique is valuable in evaluating cancers such as HN and prostate cancer,<sup>88,89</sup> where early response indicators could be crucial. Quantitative assessment of T1 and T2 relaxation times shows promise in predicting prostate radiation therapy response.<sup>90</sup> Chemical exchange saturation transfer MRI can quantify chemical components, with amide proton transfer helping distinguish true progression from pseudoprogression in glioma.<sup>91</sup> These quantitative MRI tools provide valuable noninvasive insights into tissue function, structure, and physiology, revealing tumor heterogeneity, hypoxia characteristics, and treatment

response. All this information helps identify heterogeneous targets and support the feasibility of dose escalation in more aggressive or radioresistant disease areas.

Rapid MRI techniques are essential to achieve comprehensive quantitative measurement. Emerging fast MRI techniques significantly reduce imaging acquisition times through advanced reconstruction algorithms for sparsity acquisitions, such as parallel imaging and compressed sensing.92,93 MR fingerprinting, a novel, ultrafast quantitative method, enables simultaneous measurement of multiple parameters, demonstrating great potential for distinguishing diverse tissue characteristics.94-97 Moreover, AI and ML are increasingly being adopted to accelerate MRI reconstruction.98,99

Online adaptive MRIgRT transforms the conventional workflow in radiation therapy, introducing many intensive tasks requiring AI assistance for time saving without compromising the treatment accuracy during daily treatment.<sup>100-103</sup> Additionally, accurate dose accumulation over daily treatments requires robust DIR and precise dose-mapping methods, both of which can also benefit from advancements in AI techniques. Real voxel-by-voxel daily dose assessments enable continuous tracking therapeutic doses for targets and normal tissue tolerances, providing valuable data to further guide future treatments.69,70

It is worth mentioning that the true potential of MRgRT is not merely the increase in target coverage and reduction of toxicity, which may likely improve clinical outcomes for local control and survival rate. More importantly, it opens opportunities to address complex scenarios, such as ultra-dose escalation in areas with large motion or cases in close proximity to critical organs, and reirradiated tumors, among others, that might have otherwise been impossible to treat.<sup>76,104</sup>

## Conclusion

CBCT-based and MRI-based online ART have gained increasing adoption due to their ability to address daily anatomical variations that are difficult to account for with conventional RT. Given the significant efforts from manufacturers and leading academic centers to advance online ART, we anticipate broader adoption of online ART (potentially even real-time ART) in the near future. However, implementing these technologies remains costly and time-intensive. Therefore, a strategic approach for careful patient selection is essential to ensure that the selected patients could benefit most from online ART and that resources are effectively utilized.

#### References

1) Yan D, Vicini F, Wong J, Martinez A. Adaptive radiation therapy. *Phys Med Biol.* 1997;42(1):123-132. doi:10.1088/0031-9155/42/ 1/008

2) Kishan AU, Cui J, Wang P-C, et al. Quantification of gross tumour volume changes between simulation and first day of radiotherapy for patients with locally advanced malignancies of the lung and head/neck. *J Med Imaging Radiat Oncol.* 2014;58(5):618-624. doi:10.1111/1754-9485.12196

3) Cai B, Laugeman E, Mazur TR, et al. Characterization of a prototype rapid kilovoltage x-ray image guidance system designed for a ring shape radiation therapy unit. *Med Phys.* 2019;46(3):1355-1370. doi:10. 1002/mp.13396

4) Robar JL, Cherpak A, MacDonald RL, et al. Novel technology allowing cone beam computed tomography in 6 seconds: A patient study of comparative image quality. *Pract Radiat Oncol.* 2024;14(3):277-286. doi:10. 1016/j.prro.2023.10.014

5) Kim E, Park YK, Zhao T, et al. Image quality characterization of an ultra-highspeed kilovoltage cone-beam computed tomography imaging system on an O-ring linear accelerator. *J Appl Clin Med Phys*. 2024;25(5):e14337. doi:10.1002/acm2.14337 6) Mutic S, Dempsey JF. The viewray system: magnetic resonance-guided and controlled radiotherapy. *Semin Radiat Oncol.* 2014;24(3):196-199. doi:10.1016/ j.semradonc.2014.02.008

7) Liney GP, Whelan B, Oborn B, Barton M, Keall P. MRI-linear accelerator radiotherapy systems. *Clin Oncol (R Coll Radiol)*. 2018;30(11):686-691. doi:10.1016/j.clon.2018. 08.003

8) Piperdi H, Portal D, Neibart SS, et al. Adaptive radiation therapy in the treatment of lung cancer: an overview of the current state of the field. *Front Oncol.* 2021;11:770382. doi:10.3389/fonc.2021.770382

9) Glide-Hurst CK, Lee P, Yock AD, et al. Adaptive Radiation Therapy (ART) strategies and technical considerations: A state of the ART review from NRG oncology. *Int J Radiat Oncol Biol Phys.* 2021;109(4):1054-1075. doi:10. 1016/j.ijrobp.2020.10.021

10) Green OL, Henke LE, Hugo GD. Practical clinical workflows for online and offline adaptive radiation therapy. *Semin Radiat Oncol.* 2019;29(3):219-227. doi:10.1016/ j.semradonc.2019.02.004

11) Vargas C, Yan D, Kestin LL, et al. Phase II dose escalation study of image-guided adaptive radiotherapy for prostate cancer: use of dose-volume constraints to achieve rectal isotoxicity. *Int J Radiat Oncol Biol Phys.* 2005;63(1):141-149. doi:10.1016/j.ijrobp. 2004.12.017

12) Vargas C, Martinez A, Kestin LL, et al. Dose-volume analysis of predictors for chronic rectal toxicity after treatment of prostate cancer with adaptive imageguided radiotherapy. *Int J Radiat Oncol Biol Phys.* 2005;62(5):1297-1308. doi:10.1016/j. ijrobp.2004.12.052

13) Schwartz DL, Garden AS, Thomas J, et al. Adaptive radiotherapy for head-andneck cancer: initial clinical outcomes from a prospective trial. *Int J Radiat Oncol Biol Phys.* 2012;83(3):986-993. doi:10.1016/j.ijrobp. 2011.08.017

14) Morgan HE, Wang K, Yan Y, et al. Preliminary evaluation of PTV margins for online adaptive radiation therapy of the prostatic fossa. *Pract Radiat Oncol.* 2023;13(4):e345-e353. doi:10.1016/j.prro.2022. 11.003

15) Feng M, Kong F-M, Gross M, et al. Using fluorodeoxyglucose positron emission tomography to assess tumor volume during radiotherapy for non-small-cell lung cancer and its potential impact on adaptive dose escalation and normal tissue sparing. *Int J Radiat Oncol Biol Phys.* 2009;73(4):1228-1234. doi:10.1016/j.ijrobp.2008.10.054

16) Xiao L, Liu N, Zhang G, et al. Late-course adaptive adjustment based on metabolic tumor volume changes during radiotherapy may reduce radiation toxicity in patients with non-small cell lung cancer. *PLOS ONE*. 2017;12(1):e0170901. doi:10.1371/ journal.pone.0170901 17) Yan D, Chen S, Krauss DJ, et al. Tumor voxel dose-response matrix and dose prescription function derived using <sup>18</sup>f-FDG PET/CT images for adaptive dose painting by number. *Int J Radiat Oncol Biol Phys.* 2019;104(1):207-218. doi:10.1016/j. ijrobp.2019.01.077

18) Matuszak MM, Kashani R, Green M, et al. Functional adaptation in radiation therapy. *Semin Radiat Oncol.* 2019;29(3):236-244. doi: 10.1016/j.semradonc.2019.02.006

19) Lalondrelle S, Huddart R. Improving radiotherapy for bladder cancer: an opportunity to integrate new technologies. *Clin Oncol (R Coll Radiol)*. 2009;21(5):380-384. doi:10.1016/j.clon.2009.03.005

20) Xia P, Qi P, Hwang A, et al. Comparison of three strategies in management of independent movement of the prostate and pelvic lymph nodes. *Med Phys.* 2010;37(9):5006-5013. doi:10.1118/1.3480505

21) Murthy V, Master Z, Adurkar P, et al. "Plan of the day" adaptive radiotherapy for bladder cancer using helical tomotherapy. *Radiother Oncol.* 2011;99(1):55-60. doi:10. 1016/j.radonc.2011.01.027

22) Webster GJ, Stratford J, Rodgers J, et al. Comparison of adaptive radiotherapy techniques for the treatment of bladder cancer. *Br J Radiol*. 2013;86(1021):20120433. doi:10.1259/bjr.20120433

23) Shelley CE, Barraclough LH, Nelder CL, Otter SJ, Stewart AJ. Adaptive radiotherapy in the management of cervical cancer: review of strategies and clinical implementation. *Clin Oncol (R Coll Radiol)*. 2021;33(9):579-590. doi:10.1016/j.clon.2021.06.007

24) Sonke JJ, Aznar M, Rasch C. Adaptive radiotherapy for anatomical changes. *Semin Radiat Oncol.* 2019;29(3):245-257. doi:10.1016/ j.semradonc.2019.02.007

25) Bertholet J, Anastasi G, Noble D, et al. Patterns of practice for adaptive and real-time radiation therapy (POP-ART RT) part II: offline and online plan adaption for interfractional changes. *Radiother Oncol.* 2020;153:88-96. doi:10.1016/j.radonc.2020.06. 017

26) Sibolt P, Andersson L, Calmels L, et al. Results of a pilot study on online adaptive radiotherapy of bladder cancer with artificial intelligence-driven full re-optimization on the anatomy of the day. *Int J Radiat Oncol Biol Phys.* 2020;108(3):S79-S80. doi:10.1016/j. ijrobp.2020.07.2231

27) de Jong R, Visser J, van Wieringen N, et al. Feasibility of conebeam CT-based online adaptive radiotherapy for neoadjuvant treatment of rectal cancer. *Radiat Oncol.* 2021;16(1):136. doi:10.1186/s13014-021-01866-7

28) Hall WA, Paulson E, Li XA, et al. Magnetic resonance linear accelerator technology and adaptive radiation therapy: an overview for clinicians. *CA Cancer J Clin.* 2022;72(1):34-56. doi:10.3322/caac.21707 29) Åström LM, Behrens CP, Calmels L, et al. Online adaptive radiotherapy of urinary bladder cancer with full re-optimization to the anatomy of the day: initial experience and dosimetric benefits. *Radiotherapy and Oncology*. 2022;171:37-42. doi:10.1016/j. radonc.2022.03.014

30) Hunt A, Hanson I, Dunlop A, et al. Feasibility of magnetic resonance guided radiotherapy for the treatment of bladder cancer. *Clin Transl Radiat Oncol.* 2020;25:46-51. doi:10.1016/j.ctro.2020.09.002

31) Intven MPW, de Mol van Otterloo SR, Mook S, et al. Online adaptive MR-guided radiotherapy for rectal cancer; feasibility of the workflow on a 1.5t MR-linac: clinical implementation and initial experience. *Radiother Oncol.* 2021;154:172-178. doi:10. 1016/j.radonc.2020.09.024

32) Keall P, Poulsen P, Booth JT. See, think, and act: real-time adaptive radiotherapy. *Semin Radiat Oncol.* 2019;29(3):228-235. doi: 10.1016/j.semradonc.2019.02.005

33) Liu PZY, Dong B, Nguyen DT, et al. First experimental investigation of simultaneously tracking two independently moving targets on an MRI-linac using real-time MRI and MLC tracking. *Med Phys.* 2020;47(12):6440-6449. doi:10.1002/mp.14536

34) Archambault Y, Boylan C, Bullock D, et al. Making on-line adaptive radiotherapy possible using artificial intelligence and machine learning for efficient daily re-planning. *Med Phys Int J.* 2020;8.

35) Yoon SW, Lin H, Alonso-Basanta M, et al. Initial evaluation of A novel cone-beam CT-based semi-automated online adaptive radiotherapy system for head and neck cancer treatment - A timing and automation quality study. *Cureus*. 2020;12(8):e9660. doi: 10.7759/cureus.9660

36) Sibolt P, Andersson LM, Calmels L, et al. Clinical implementation of artificial intelligence-driven cone-beam computed tomography-guided online adaptive radiotherapy in the pelvic region. *Phys Imaging Radiat Oncol.* 2021;17:1-7. doi: 10.1016/j.phro.2020.12.004

37) Stanley DN, Harms J, Pogue JA, et al. A roadmap for implementation of kv-CBCT online adaptive radiation therapy and initial first year experiences. *J Appl Clin Med Phys.* 2023;24(7):e13961. doi:10.1002/acm2.13961

38) Schiff JP, Stowe HB, Price A, et al. In silico trial of Computed Tomography-Guided Stereotactic Adaptive Radiation Therapy (CT-STAR) for the treatment of abdominal oligometastases. Int J Radiat Oncol Biol Phys. 2022;114(5):1022-1031. doi:10.1016/ j.ijrobp.2022.06.078

39) Dohopolski M, Choi B, Meng B, et al. Dosimetric impact of simulated daily adaptive radiotherapy with significantly reduced setup margins in the definitive treatment of head and neck cancer. *Int J Radiat Oncol Biol Phys.* 2022;114(3):e590. doi: 10.1016/j.ijrobp.2022.07.2273 40) Moazzezi M, Rose B, Kisling K, Moore KL, Ray X. Prospects for daily online adaptive radiotherapy via ethos for prostate cancer patients without nodal involvement using unedited CBCT auto-segmentation. *J Appl Clin Med Phys.* 2021;22(10):82-93. doi:10.1002/ acm2.13399

41) De Roover R, Crijns W, Poels K, et al. Automated treatment planning of prostate stereotactic body radiotherapy with focal boosting on a fast-rotating O-ring linac: plan quality comparison with C-arm linacs. *J Appl Clin Med Phys.* 2021;22(9):59-72. doi:10.1002/ acm2.13345

42) Zwart LGM, Ong F, Ten Asbroek LA, et al. Cone-beam computed tomography-guided online adaptive radiotherapy is feasible for prostate cancer patients. *Phys Imaging Radiat Oncol.* 2022;22:98-103. doi:10.1016/j. phro.2022.04.009

43) Byrne M, Archibald-Heeren B, Hu Y, et al. Varian ethos online adaptive radiotherapy for prostate cancer: early results of contouring accuracy, treatment plan quality, and treatment time. *J Appl Clin Med Phys.* 2022;23(1):e13479. doi:10.1002/ acm2.13479

44) Schiff JP, Price AT, Stowe HB, et al. Simulated computed tomographyguided stereotactic adaptive radiotherapy (CT-STAR) for the treatment of locally advanced pancreatic cancer. *Radiother Oncol.* 2022;175:144-151. doi:10.1016/j.radonc.2022. 08.026

45) Hu Y, Byrne M, Archibald-Heeren B, et al. Validation of the preconfigured varian ethos acuros XB beam model for treatment planning dose calculations: A dosimetric study. *J Appl Clin Med Phys.* 2020;21(12):27-42. doi:10.1002/acm2.13056

46) Lin J, Chen M, Lai Y, et al. ART2Dose: A comprehensive dose verification platform for online adaptive radiotherapy. *Med Phys.* 2024;51(1):18-30. doi:10.1002/mp.16806

47) Perrier L, Balusson F, Morelle M, et al. Cost-effectiveness of weekly adaptive radiotherapy versus standard IMRT in head and neck cancer alongside the ARTIX trial. *Radiother Oncol.* 2024;193:110116. doi: 10.1016/j.radonc.2024.110116

48) Raaymakers BW, Lagendijk JJW, Overweg J, et al. Integrating a 1.5 T MRI scanner with a 6 MV accelerator: proof of concept. *Phys Med Biol.* 2009;54(12):N229-37. doi:10.1088/0031-9155/54/12/N01

49) Raaymakers BW, Jürgenliemk-Schulz IM, Bol GH, et al. First patients treated with a 1.5 T MRI-linac: clinical proof of concept of a high-precision, high-field MRI guided radiotherapy treatment. *Phys Med Biol.* 2017;62(23):L41-L50. doi:10.1088/1361-6560/aa9517

50) Fallone BG. The rotating biplanar linac-magnetic resonance imaging system. *Semin Radiat Oncol.* 2014;24(3):200-202. doi: 10.1016/j.semradonc.2014.02.011 51) Keall PJ, Barton M, Crozier S. The Australian magnetic resonance imaging-linac program. *Semin Radiat Oncol.* 2014;24(3):203-206. doi:10.1016/j. semradonc.2014.02.015

52) Chuong MD, Clark MA, Henke LE, et al. Patterns of utilization and clinical adoption of 0.35 tesla MR-guided radiation therapy in the united states - understanding the transition to adaptive, ultra-hypofractionated treatments. *Clin Transl Radiat Oncol.* 2023;38:161-168. doi:10. 1016/j.ctro.2022.11.013

53) Keall PJ, Brighi C, Glide-Hurst C, et al. Integrated MRI-guided radiotherapy opportunities and challenges. *Nat Rev Clin Oncol.* 2022;19(7):458-470. doi:10.1038/s41571-022-00631-3

54) Winkel D, Bol GH, Kroon PS, et al. Adaptive radiotherapy: the elekta unity MR-linac concept. *Clin Transl Radiat Oncol.* 2019;18:54-59. doi:10.1016/j.ctro.2019.04.001

55) Keall PJ, Glide-Hurst CK, Cao M, et al. ICRU REPORT 97: MRI-guided radiation therapy using MRI-linear accelerators. *Journal of the ICRU*. 2022;22(1):1-100. doi:10. 1177/14736691221141950

56) Klüter S. Technical design and concept of a 0.35 T MR-linac. *Clin Transl Radiat Oncol.* 2019;18:98-101. doi:10.1016/j.ctro.2019.04.007

57) Dunlop A, Mitchell A, Tree A, et al. Daily adaptive radiotherapy for patients with prostate cancer using a high field MR-linac: initial clinical experiences and assessment of delivered doses compared to a C-arm linac. *Clin Transl Radiat Oncol.* 2020;23:35-42. doi: 10.1016/j.ctro.2020.04.011

58) Winkel D, Bol GH, Werensteijn-Honingh AM, et al. Target coverage and dose criteria based evaluation of the first clinical 1.5T MR-linac SBRT treatments of lymph node oligometastases compared with conventional CBCT-linac treatment. *Radiother Oncol.* 2020;146:118-125. doi:10.1016/j.radonc.2020. 02.011

59) Finazzi T, Haasbeek CJA, Spoelstra FOB, et al. Clinical outcomes of stereotactic MR-guided adaptive radiation therapy for high-risk lung tumors. *Int J Radiat Oncol Biol Phys.* 2020;107(2):270-278. doi:10.1016/j. ijrobp.2020.02.025

60) Henke LE, Contreras JA, Green OL, et al. Magnetic Resonance Image-Guided Radiotherapy (MRIgRT): A 4.5-year clinical experience. *Clin Oncol (R Coll Radiol)*. 2018;30(11):720-727. doi:10.1016/j.clon.2018. 08.010

61) Aluwini S, Pos F, Schimmel E, et al. Hypofractionated versus conventionally fractionated radiotherapy for patients with prostate cancer (HYPRO): acute toxicity results from a randomised non-inferiority phase 3 trial. *Lancet Oncol.* 2015;16(3):274-283. doi:10.1016/S1470-2045(14)70482-6 62) Bruynzeel AME, Tetar SU, Oei SS, et al. A prospective single-arm phase 2 study of stereotactic magnetic resonance guided adaptive radiation therapy for prostate cancer: early toxicity results. *Int J Radiat Oncol Biol Phys.* 2019;105(5):1086-1094. doi:10. 1016/j.ijrobp.2019.08.007

63) Dearnaley D, Syndikus I, Mossop H, et al. Conventional versus hypofractionated high-dose intensity-modulated radiotherapy for prostate cancer: 5-year outcomes of the randomised, non-inferiority, phase 3 chhip trial. *Lancet Oncol.* 2016;17(8):1047-1060. doi: 10.1016/S1470-2045(16)30102-4

64) El-Bared N, Portelance L, Spieler BO, et al. Dosimetric benefits and practical pitfalls of daily online adaptive MRI-guided stereotactic radiation therapy for pancreatic cancer. *Pract Radiat Oncol.* 2019;9(1):e46-e54. doi:10.1016/j.prro.2018.08.010

65) Henke L, Kashani R, Robinson C, et al. Phase I trial of stereotactic MR-guided online adaptive radiation therapy (SMART) for the treatment of oligometastatic or unresectable primary malignancies of the abdomen. *Radiother Oncol.* 2018;126(3):519-526. doi:10. 1016/j.radonc.2017.11.032

66) Tetar SU, Bruynzeel AME, Lagerwaard FJ, et al. Clinical implementation of magnetic resonance imaging guided adaptive radiotherapy for localized prostate cancer. *Phys Imaging Radiat Oncol.* 2019;9:69-76. doi: 10.1016/j.phro.2019.02.002

67) Crane CH, O'Reilly EM. Ablative radiotherapy doses for Locally Advanced: Pancreatic Cancer (LAPC). *Cancer J.* 2017;23(6):350-354. doi:10.1097/PPO. 000000000000292

68) Finazzi T, van Sörnsen de Koste JR, Palacios MA, et al. Delivery of magnetic resonance-guided single-fraction stereotactic lung radiotherapy. *Phys Imaging Radiat Oncol.* 2020;14:17-23. doi:10.1016/j.phro.2020.05.002

69) Borman PTS, Bos C, Stemkens B, et al. Assessment of 3D motion modeling performance for dose accumulation mapping on the MR-linac by simultaneous multislice MRI. *Phys Med Biol.* 2019;64(9):095004. doi:10.1088/1361-6560/ab13e3

70) Glitzner M, Crijns SPM, de Senneville BD, et al. On-line MR imaging for dose validation of abdominal radiotherapy. *Phys Med Biol.* 2015;60(22):8869-8883. doi:10.1088/0031-9155/ 60/22/8869

71) Bentzen SM, Constine LS, Deasy JO, et al. Quantitative Analyses of Normal Tissue Effects in the Clinic (QUANTEC): an introduction to the scientific issues. *Int J Radiat Oncol Biol Phys.* 2010;76(3 suppl):S3-9. doi:10.1016/j.ijrobp.2009.09.040

72) Marks LB, Yorke ED, Jackson A, et al. Use of normal tissue complication probability models in the clinic. *Int J Radiat Oncol Biol Phys.* 2010;76(3 suppl):S10-9. doi:10.1016/ j.ijrobp.2009.07.1754 73) Bonavia R, Inda M, Cavenee WK, Furnari FB. Heterogeneity maintenance in glioblastoma: a social network. *Cancer Res.* 2011;71(12):4055-4060. doi:10.1158/0008-5472. CAN-11-0153

74) Castellano A, Bailo M, Cicone F, et al. Advanced imaging techniques for radiotherapy planning of gliomas. *Cancers (Basel)*. 2021;13(5):1063):13:. doi:10. 3390/cancers13051063

75) Kim MM, Aryal MP, Sun Y, et al. Response assessment during chemoradiation using a hypercellular/hyperperfused imaging phenotype predicts survival in patients with newly diagnosed glioblastoma. *Neuro Oncol.* 2021;23(9):1537-1546. doi:10. 1093/neuonc/noab038

76) Pathmanathan AU, van As NJ, Kerkmeijer LGW, et al. Magnetic resonance imaging-guided adaptive radiation therapy: A "game changer" for prostate treatment? *Int J Radiat Oncol Biol Phys.* 2018;100(2):361-373. doi:10. 1016/j.ijrobp.2017.10.020

77) Schumacher L-E, Dal Pra A, Hoffe SE, Mellon EA. Toxicity reduction required for MRI-guided radiotherapy to be cost-effective in the treatment of localized prostate cancer. *Br J Radiol.* 2020;93(1114):20200028. doi:10. 1259/bjr.20200028

78) Tijssen RHN, Philippens MEP, Paulson ES, et al. MRI commissioning of 1.5T MR-linac systems - a multi-institutional study. *Radiother Oncol.* 2019;132:114-120. doi: 10.1016/j.radonc.2018.12.011

79) Raaijmakers AJE, Raaymakers BW, Lagendijk JJW. Integrating a MRI scanner with a 6 MV radiotherapy accelerator: dose increase at tissue-air interfaces in a lateral magnetic field due to returning electrons. *Phys Med Biol.* 2005;50(7):1363-1376. doi:10. 1088/0031-9155/50/7/002

80) Wen N, Kim J, Doemer A, et al. Evaluation of a magnetic resonance guided linear accelerator for stereotactic radiosurgery treatment. *Radiother Oncol.* 2018;127(3):460-466. doi:10.1016/j. radonc.2018.04.034

81) Weygand J, Fuller CD, Ibbott GS, et al. Spatial precision in magnetic resonance imaging-guided radiation therapy: the role of geometric distortion. *Int J Radiat Oncol Biol Phys.* 2016;95(4):1304-1316. doi:10.1016/j. ijrobp.2016.02.059

82) Campbell-Washburn AE, Ramasawmy R, Restivo MC, et al. Opportunities in interventional and diagnostic imaging by using high-performance low-field-strength MRI. *Radiology*. 2019;293(2):384-393. doi:10. 1148/radiol.2019190452

83) Bird D, Henry AM, Sebag-Montefiore D, et al. A systematic review of the clinical implementation of pelvic magnetic resonance imaging-only planning for external beam radiation therapy. *Int J Radiat Oncol Biol Phys.* 2019;105(3):479-492. doi:10. 1016/j.ijrobp.2019.06.2530

8

84) Wegener D, Thome A, Paulsen F, et al. First experience and prospective evaluation on feasibility and acute toxicity of online adaptive radiotherapy of the prostate bed as salvage treatment in patients with biochemically recurrent prostate cancer on a 1.5T MR-linac. *J Clin Med.* 2022;11(16):4651):11:. doi:10.3390/ jcm11164651

85) Weykamp F, Katsigiannopulos E, Piskorski L, et al. Dosimetric benefit of adaptive magnetic resonance-guided stereotactic body radiotherapy of liver metastases. *Cancers* (*Basel*). 2022;14(24):6041):14:. doi:10.3390/ cancers14246041

86) Cao Y. The promise of dynamic contrast-enhanced imaging in radiation therapy. *Semin Radiat Oncol.* 2011;21(2):147-156. doi:10.1016/j. semradonc.2010.11.001

87) Zahra MA, Tan LT, Priest AN, et al. Semiquantitative and quantitative dynamic contrast-enhanced magnetic resonance imaging measurements predict radiation response in cervix cancer. *Int J Radiat Oncol Biol Phys.* 2009;74(3):766-773. doi:10.1016/j. ijrobp.2008.08.023

88) Galbán CJ, Mukherji SK, Chenevert TL, et al. A feasibility study of parametric response map analysis of diffusion-weighted magnetic resonance imaging scans of head and neck cancer patients for providing early detection of therapeutic efficacy. *Transl Oncol.* 2009;2(3):184-190. doi:10.1593/ tlo.09175

89) Liu L, Wu N, Ouyang H, Dai J-R, Wang W-H. Diffusion-weighted MRI in early assessment of tumour response to radiotherapy in high-risk prostate cancer. *Br J Radiol.* 2014;87(1043):20140359. doi:10.1259/ bjr.20140359 90) Foltz WD, Wu A, Chung P, et al. Changes in apparent diffusion coefficient and T2 relaxation during radiotherapy for prostate cancer. J Magn Reson Imaging. 2013;37(4):909-916. doi:10.1002/jmri.23885

91) Ma B, Blakeley JO, Hong X, et al. Applying amide proton transfer-weighted MRI to distinguish pseudoprogression from true progression in malignant gliomas. *J Magn Reson Imaging*. 2016;44(2):456-462. doi: 10.1002/jmri.25159

92) Lustig M, Donoho D, Pauly JM. Sparse MRI: the application of compressed sensing for rapid MR imaging. *Magn Reson Med.* 2007;58(6):1182-1195. doi:10.1002/mrm.21391

93) Deshmane A, Gulani V, Griswold MA, Seiberlich N. Parallel MR imaging. *J Magn Reson Imaging*. 2012;36(1):55-72. doi:10.1002/ jmri.23639

94) Cohen O, Huang S, McMahon MT, Rosen MS, Farrar CT. Rapid and quantitative Chemical Exchange Saturation Transfer (CEST) imaging with magnetic resonance fingerprinting (MRF). *Magn Reson Med*. 2018;80(6):2449-2463. doi:10.1002/mrm.27221

95) Lu L, Chen Y, Shen C, et al. Initial assessment of 3D Magnetic Resonance Fingerprinting (MRF) towards quantitative brain imaging for radiation therapy. *Medical Physics*. 2020;47(3):1199-1214. doi:10. 1002/mp.13967

96) Ma D, Gulani V, Seiberlich N, et al. Magnetic resonance fingerprinting. *Nature*. 2013;495(7440):187-192. doi:10.1038/ nature11971

97) Yu AC, Badve C, Ponsky LE, et al. Development of a combined MR fingerprinting and diffusion examination for prostate cancer. *Radiology*. 2017;283(3):729-738. doi: 10.1148/radiol.2017161599 98) Chandra SS, Bran Lorenzana M, Liu X, et al. Deep learning in magnetic resonance image reconstruction. *J Med Imag Rad Onc.* 2021;65(5):564-577. doi:10. 1111/1754-9485.13276

99) Freedman JN, Gurney-Champion OJ, Nill S, et al. Rapid 4D-MRI reconstruction using a deep radial convolutional neural network: dracula. *Radiother Oncol.* 2021;159:209-217. doi:10.1016/j.radonc.2021.03.034

100) Owrangi AM, Greer PB, Glide-Hurst CK. MRI-only treatment planning: benefits and challenges. *Phys Med Biol.* 2018;63(5):05TR01. doi:10.1088/1361-6560/aaaca4

101) Pereira S, Pinto A, Alves V, Silva CA. Brain tumor segmentation using convolutional neural networks in MRI images. *IEEE Trans Med Imaging*. 2016;35(5):1240-1251. doi: 10.1109/TMI.2016.2538465

102) Jagt TZ, Janssen TM, Betgen A, et al. Benchmarking daily adaptation using fully automated radiotherapy treatment plan optimization for rectal cancer. *Phys Imaging Radiat Oncol.* 2022;24:7-13. doi:10. 1016/j.phro.2022.08.006

103) Künzel LA, Leibfarth S, Dohm OS, et al. Automatic VMAT planning for post-operative prostate cancer cases using particle swarm optimization: A proof of concept study. *Phys Med.* 2020;69:101-109. doi:10. 1016/j.ejmp.2019.12.007

104) Levin-Epstein R, Cao M, Lee P, et al. Magnetic resonance-guided inter-fraction monitoring opens doors to delivering safer reirradiation: an illustrative case report and discussion. *Cureus*. 2018;10(4):e2479. doi:10. 7759/cureus.2479